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## Application of Reverse Time Migration (RTM) for ultrasound tomography problem

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# **Medical diagnostics**

One of the most important problems of medical diagnostics is the early detection of a variety of breast cancer tumors.



✓ X-ray tomography (CT)

Mammography (also called mastography)

Magnetic resonance tomography (MRT)

<u>Ultrasound examinations</u> are relatively inexpensive, easy to use and safe diagnostic methods. Ultrasound imaging has great potential for the detection and diagnosis of breast cancer Nowadays groups of scientists in Russia (MSU, chair of acoustics), in the USA (N. Duric, C. Li, P. Littrup, S. Schmindt, etc.) and in Germany (N. Ruiter, R. Dapp, M. Zapf, R. Jirik, etc) work on creation of models of the ultrasonic tomographs with high resolution and informative.



However, one of the major problems is the development of effective algorithms for measurements processing, i.e. numerical methods with high resolution for acoustics inverse problems.

In order to obtain of the image of the speed of sound, we use RTM procedure (in the version [1]) for the ultrasound data.

[1] D. Rocha, N. Tanushev, P. Sava Acoustic wavefield imaging using the energy norm // 2015 SEG Annual Meeting, 18-23 October, New Orleans, Louisiana, P. 49-68



Fig. 2 Riker's impulse

#### Imaging problem

For the given boundary measurements

$$p_0(x,t;x_s) = p(x,t;x_s), x \in \Gamma, t \in [0,T]$$

it is required to find the image of the speed of sound in the domain  $\Omega$ .

Registration time of the waves - *T*, where  $T > 2T^*$ ,  $T^*$  – «acoustic» radius of domain Ω.

#### Procedure of RTM

We use a version of the known in geophysics RTM procedure proposed in [1]. RTM procedure consists of the following steps:

Step 1: We calculate the  $p_t^{air}(x,t;x_s)$ ,  $\nabla p^{for}(x,t;x_s)$ for the known acoustical medium (speed of sound  $C_0$ )

Step 2: For give  $\mathbf{p}_0(x,t;x_s)$  we solve reversal time problem:

$$\frac{1}{c_0^2} p_{tt} - \Delta p = f(t)\delta(x - x_s) \quad in \quad \Omega \times [0,T]$$
$$p \mid_{t=T} = p_t \mid_{t=T} = 0, \qquad p \mid_{\Gamma \times [0,T]} = p_0$$

 $p^{back}(x,t;x_s)$  the solution of this problem Step 3: We use the imaging condition

$$I_E(x) = \sum_{s} \int_{0}^{T} [p_t^{for} p_t^{back} + (\nabla p^{for}, \nabla p^{back})]dt$$

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#### Numerical experiment



Fig. 3 Scheme of the experiment

Parameters of the experiment:

The number of nodes 10 240 000

dx = 0.1 mm.Radiats (domain  $\Omega$ ) 15 cm



Parameters of ultrasound tomography:

The radius of the membrane 15 sm.

The number of transducers 256

The dominant frequency of the impulse 1.3  $M\Gamma\mu$ 



Fig. 4– Complicated acoustic model

Sandhu GY., Li C., Roy O., Schmidt S., Duric N. Frequency domain ultrasound waveform tomography: breast imaging using a ring transducer // Physics in Medicine & Biology. 2015. 60, P. 5381-5398

#### Numerical experiment, RTM



Fig. 5-RTM for complicated acoustic model

Step 1: We recover the boundary indicated by the letter "K" in Fig. 4. For this we apply RTM procedure for a «small» time T (fig. 6).



Fig. 6 - Image of speed of sound for a short time of observation

Step 2. We continue in reverse time wavefield and get wavefield denoted by at the poundary (Fig. 7). So we overcome through the boundary "K".



Fig. 7 - Complicated acoustic model, scheme of the boundary  $\Gamma_1$  location.

## Step 3. We apply RTM procedure for data inclusions (Fig. 8)

#### and get the image of



Fig. 8- The image of the speed of sound.

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## THANK YOU FOR YOUR ATTENTION!